

# **Propagation Phase Contrast Imaging For Angiography**

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# Introduction

- Imaging from X-rays is of great importance today
- 1895 - Wilhelm Röntgen
- Good image quality is related to good diagnoses
- New techniques as X-Pci have been developed
- These have brought advances in different areas



**Figura 1.** Mano de la esposa de Wilhelm Röntgen  
Imagen tomada de: Röntgen, W (1896) *On a new kind of rays.* Science, Vol 111, No. 59

# X Ray imaging

## X ray attenuation imaging

- Wave intensity decays. It follows Beer-Lambert law (1)

$$(1) \quad I = I_0 e^{-\mu t}$$

- $\mu$ : Linear attenuation coefficient
- $t$ : Sample thickness

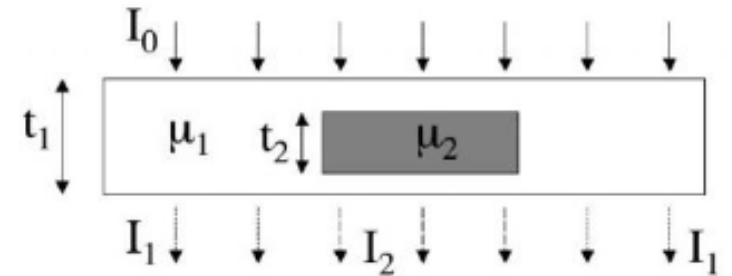
# X Ray imaging

## X ray attenuation imaging

$$(2) I_1 = I_0 e^{-\mu_1 t_1} \quad (3) I_2 = I_0 e^{-\mu_1(t_1-t_2)} e^{-\mu_2 t_2}$$

- Contrast attenuation is defined by intensity differences.

$$(4) C_{att} = \frac{I_1 - I_2}{I_1} = 1 - e^{-(\mu_1 - \mu_2)t_2}$$



**Figura 2.** Intensities after passing through samples with different attenuation coefficients and thicknesses.

Image taken from: Olivo, A and Castelli, E. (2014) *X-ray phase contrast imaging: From synchrotrons to conventional sources*, La Rivista del Nuovo Cimento, Vol 37

# X Ray imaging

## X ray attenuation imaging

- Three dimension generalization:

$$(5) \quad I(x, y) = I_0(x, y)e^{-(\mu_1^\lambda - \mu_2^\lambda)T_0(x, y)}$$

$$(6) \quad T(x) = 2\sqrt{r^2 - x^2}$$

$$(7) \quad I(x, y) = \int I_0(x, y)e^{-(\mu_1^\lambda - \mu_2^\lambda)T_0(x, y)} D(\lambda)d\lambda$$

# X Ray imaging

## X Ray phase contrast imaging

- Phase shift of X-rays as they pass through a certain sample

$$(8) \quad \Psi_i(\mathbf{r}, t) = E_0(\mathbf{r})e^{-i\omega t}$$

- X-rays induce oscillations on electrons

$$(9) \quad f = \frac{-\omega^2}{(\omega^2 - \omega_0^2 - i\Gamma\omega)} = -(f' + f'')$$

# X Ray imaging

## X Ray phase contrast imaging

- An index of refraction is defined which in turn is complex

$$(10) \quad n = 1 - r_e(N\lambda^2/2\pi)$$

$$(11) \quad n = 1 - \delta + i\beta$$

$$(12) \quad \Phi = \frac{2\pi}{\lambda} \int_{Superficie} \delta(x, y, z) dz$$

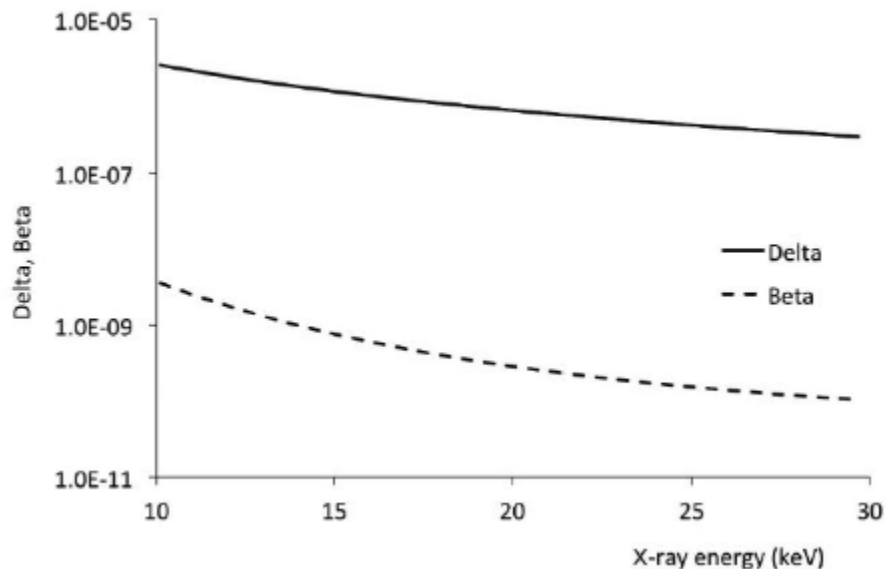
$$(13) \quad \mu = \frac{4\pi\beta}{\lambda} = \frac{2\omega\beta}{c} = 2N\lambda r_e f''$$

# X Ray imaging

## X Ray phase contrast imaging

- The scattered wave will have the form :

$$(12) \quad \Psi_r(\mathbf{r}, t) = E_0(\mathbf{r}) \exp\left(\frac{2\pi i n l}{\lambda}\right) = \Psi_0 \exp\left(\frac{2\pi i \delta l}{\lambda}\right) \exp\left(\frac{-2\pi i \beta l}{\lambda}\right)$$



**Figura 3.**  $\delta$  and  $\beta$  coefficients in a 10 – 30 keV energy range for PMMA. Image taken from: Olivo, A and Castelli, E. (2014) *X-ray phase contrast imaging: From synchrotrons to conventional sources*, La Rivista del Nuovo Cimento, Vol 37



# X Ray imaging

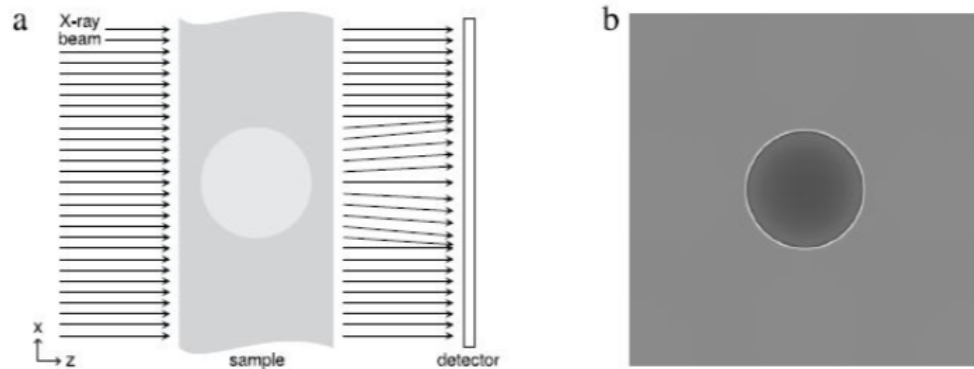
## X Ray phase contrast imaging

- An increased intensity is detected on the edges of the sample

- A new contrast is defined:

$$(13) C_{phase} = \frac{I_{max} - I_{min}}{I_{Background}}$$

$$(14) CNR = \frac{I_{Max} - I_{Background}}{\sigma_{Background}}$$



**Figura 4.** XRPCi Representation: (a) Sample plane (b) Image obtained represented as an intensity distribution. Image taken from: M. Endrizzi. (2017) *X-ray phase contrast imaging*, Nuclear Inst. and Methods in Physics Research, Vol 878

# XPCi Methods

There are 5 main methods to execute XPCi

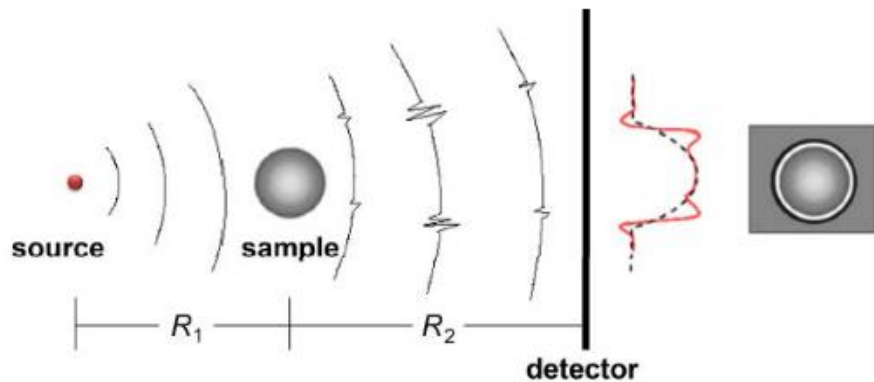
These are:

- Interferometry method
- Free-space propagation/ propagation based imaging/ In line Pci
- Analyzer based imaging (Diffraction Enhanced imaging)
- Grating based imaging
- Tracking based methods

Some others derive from these, like Edge Illumination

# Free space propagation

- Easier and cheaper way to execute XPCi
- Requires a great space between sample and detector
- The greater the space, the greater the phase shift effects
- Intensity changes are given by phase shifts



**Figura 9.** In-Line Pci squematic representation. Image taken from: X. Guo et al (2011) *Improving image qualityof x-ray in-line phase contrast imaging using an image restoration method*, Optic Express, Vol 19, No 23

# Free space propagation

- Intensity distribution in (x,y) plane is given by:

$$(15) \quad I(x, y, M, \lambda) = \frac{I_0}{M^2} \left( 1 + \frac{R_2 \lambda}{2\pi M} \nabla^2 \phi(x, y, R_1, \lambda) \right)$$

$$(16) \quad M = \frac{R_1 + R_2}{R_1}$$

- A high spatial coherence is required

$$(17) \quad l_c = \frac{\lambda R_1}{\sigma_s 2\sqrt{2 \log 2}}$$

# Free space propagation

- Its use dates back to 1995 by Snigrev et al [34].
- Point sources and synchrotron sources have been used [36,37].
- In the investigative part, the following stand out:
  1. Holotomographies [38].
  2. Tomographies [39].
  3. Coronary arteries visualization [44].
  4. Collagen fibers [46].
  5. Rodent lungs [50].
  6. etc

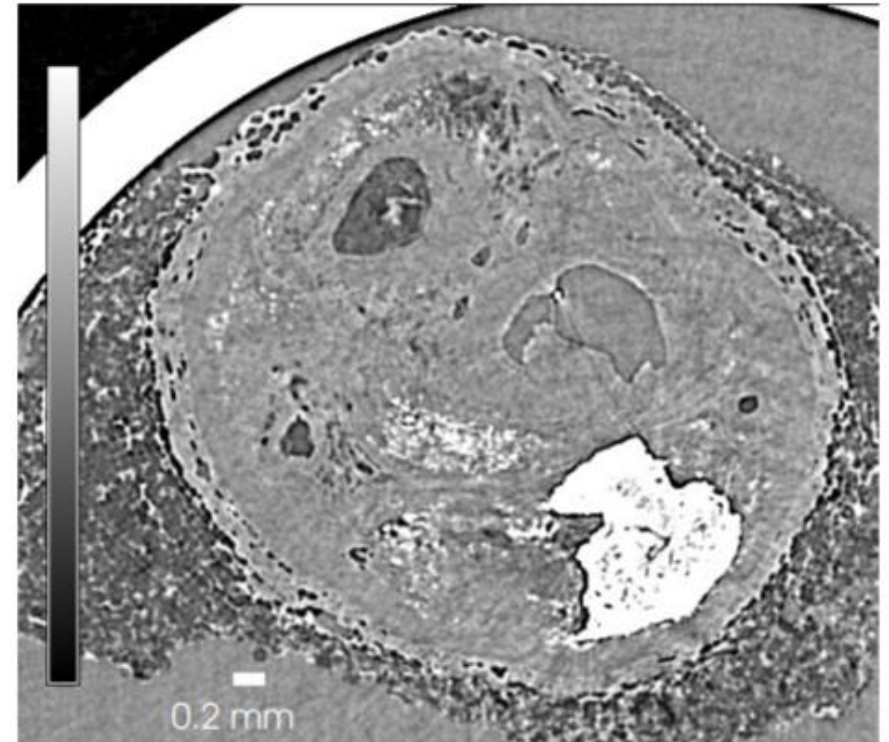
# State of Art

## XPCi angiography:

### In-line holography and phase-contrast microtomography with high energy x-rays

P Spanne, C Raven, I Snigireva and A Snigirev†  
European Synchrotron Radiation Facility, BP 220, F-38043 Grenoble Cedex, France

- 5.1 mm external diameter artery.
- Sample at 66 cm from the X ray source.
- Source energy: 28 keV.
- Increased intensity at the edges.



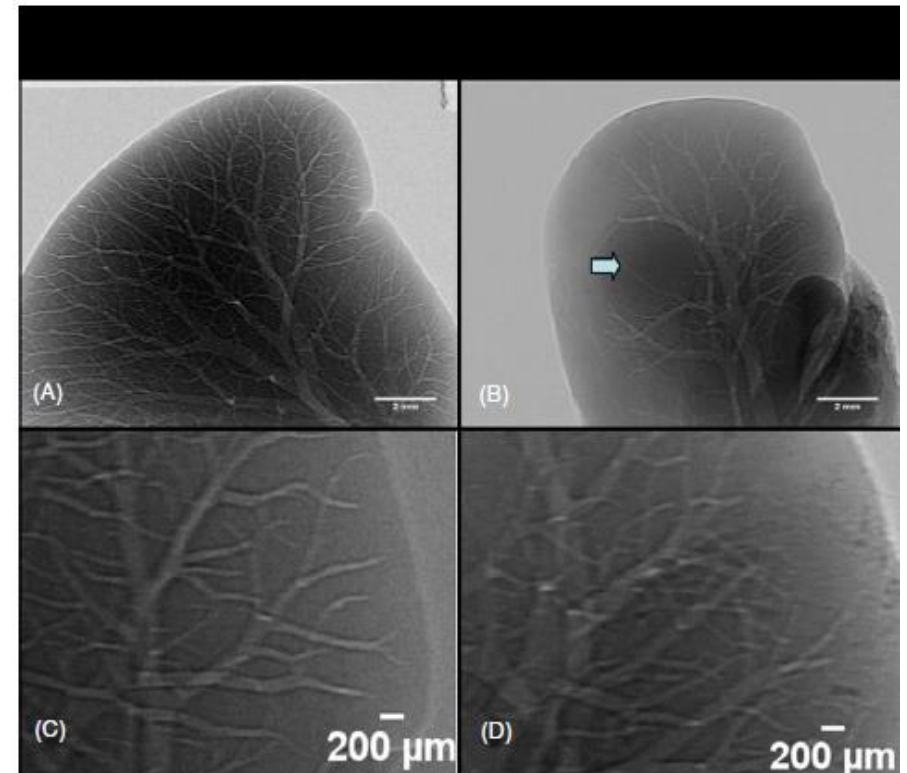
# State of Art

## XPCi angiography:

### Mouse blood vessel imaging by in-line x-ray phase-contrast imaging

Xi Zhang<sup>1</sup>, Xiao-Song Liu<sup>3</sup>, Xin-Rong Yang<sup>2</sup>, Shao-Liang Chen<sup>1,4</sup>,  
Pei-Ping Zhu<sup>3</sup> and Qing-Xi Yuan<sup>3</sup>

- Visualization of 200  $\mu\text{m}$  arteries in kidneys.
- Absence of contrast agents.



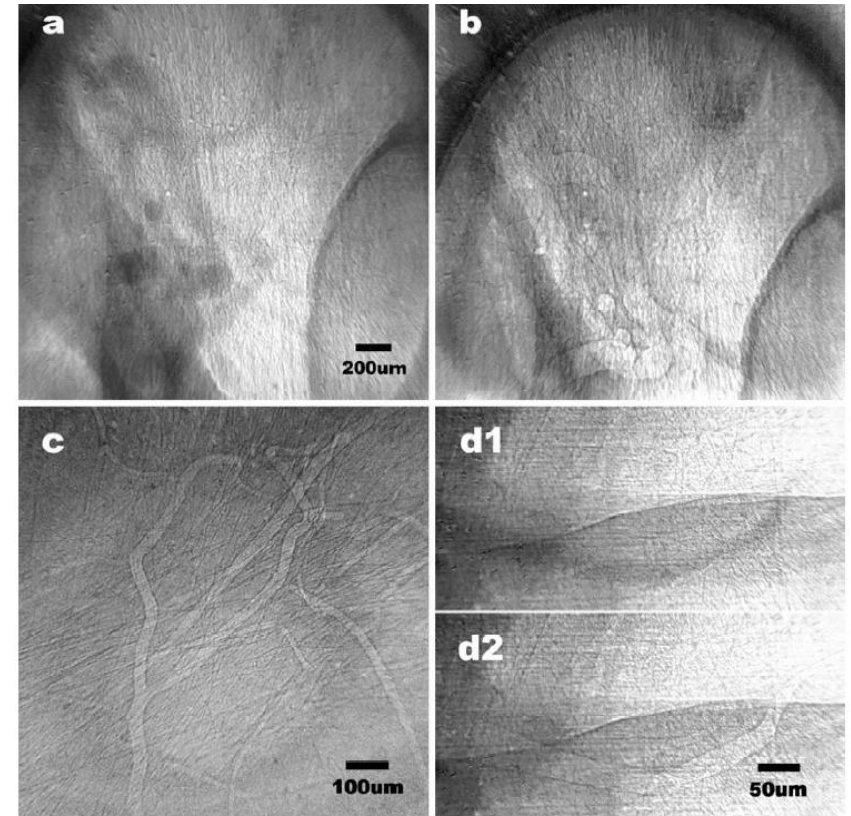
# State of Art

XPCi angiography:

Synchrotron microangiography with no contrast agent

Y Hwu<sup>1</sup>, W L Tsai<sup>1</sup>, J H Je<sup>2</sup>, S K Seol<sup>2</sup>, Bora Kim<sup>2</sup>, A Groso<sup>3</sup>,  
G Margaritondo<sup>3</sup>, Kyu-Ho Lee<sup>4</sup> and Je-Kyung Seong<sup>4</sup>

- 8  $\mu\text{m}$  arteries
- Presence of contrast agents.





# McXtrace

- X Ray simulator
- Based on Monte Carlo (MC) methods
- Quantitative and qualitative data

**McXtrace - Monte Carlo Xray Tracing, is a joint venture by**



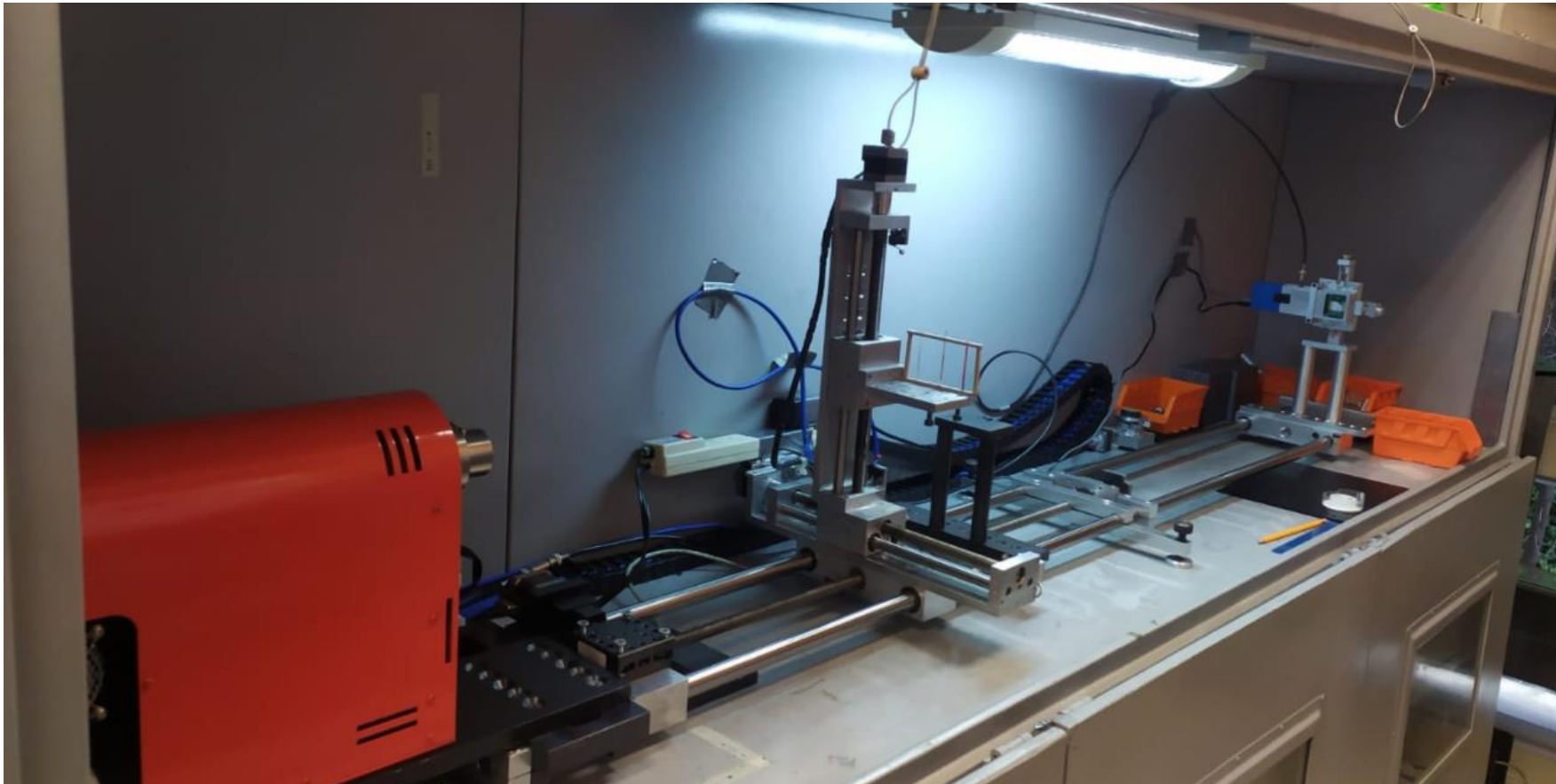
The image displays the logos of the four institutions involved in the joint venture: DTU (Technical University of Denmark), ESRF (European Synchrotron Radiation Facility), SAXSLAB GANESHA (Synchrotron X-ray Analysis and Scattering Laboratory at GANESHA), and McStas (Monte Carlo Simulation of X-ray Scattering). The McStas logo features a blue circle with a yellow 'n' and an arrow pointing to the right.

Our code is based on technology from

**Figura 14.** McXtrace. Imagen taken from: <https://www.mcxtrace.org/>

# Experimental set-up

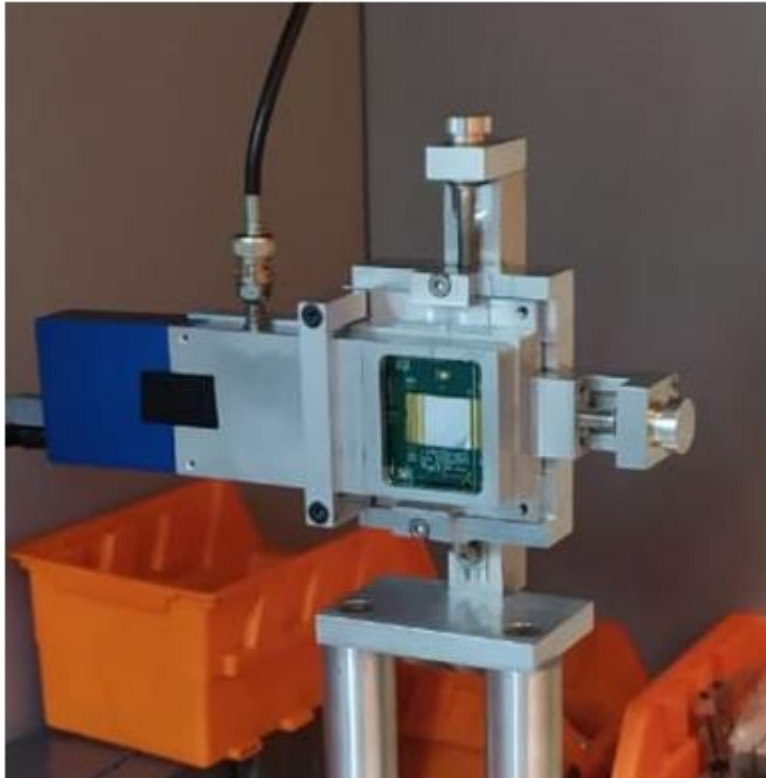
- Hamamatsu L6622-01 with colimator
- Medipix 3RXV1
- Sample



**Figura 14.** Experimental set-up

# Experimental set-up

X Ray detector: Medipix 3RXV1



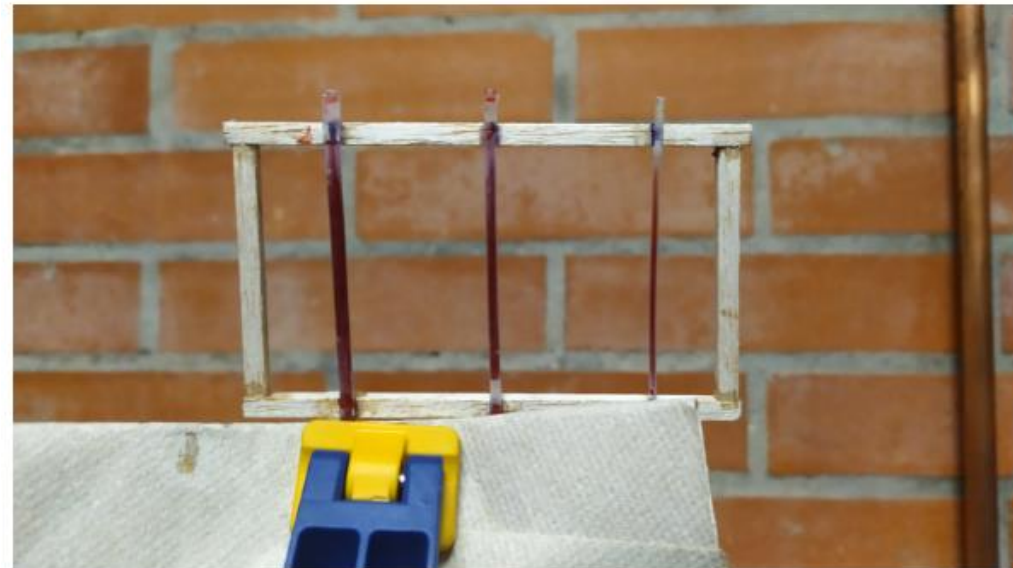
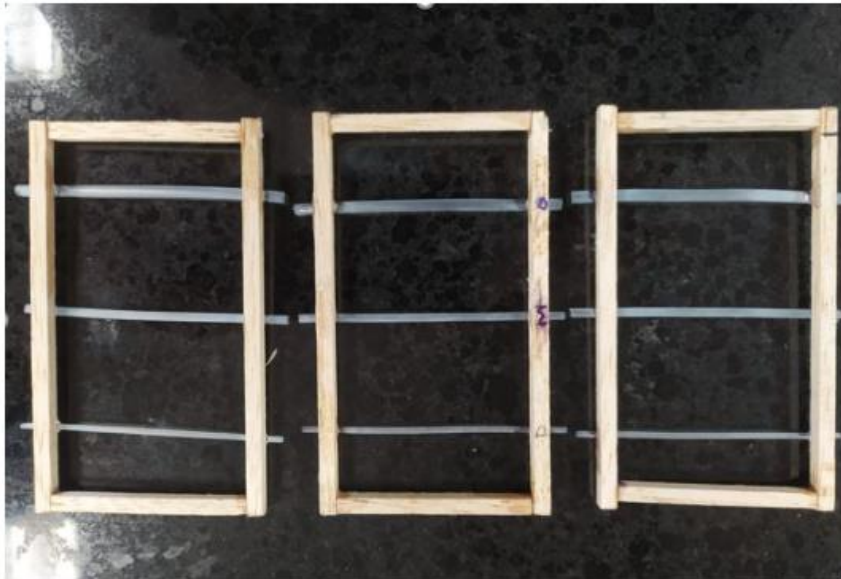
- Silicon
- 256 x 256 pixels matrix
- 55  $\mu\text{m}$
- -100 V
- 10  $\mu\text{A}$
- 1.8 m from the source

**Figura 16** Medipix 3RXV1 X Ray detector

# Samples

## Artificial Sample

- Catheter PVC sample tubes of 1.43, 2.00 and 2.54 mm external diameter
- They have been filled with air, povidone iodine and beef blood
- 0.6 m from the source



**Figura 17.** Samples designed for the experimental set-up

# Samples

## Organic Sample

- Pig pulmonary aorta
- Filled with air, povidone iodine and beef blood



• **Figura 18.** Pig pulmonary aorta

# Simulated set-up

- X-ray point source
- Pixel matrix as detector
- Sample: Concentric cylinders

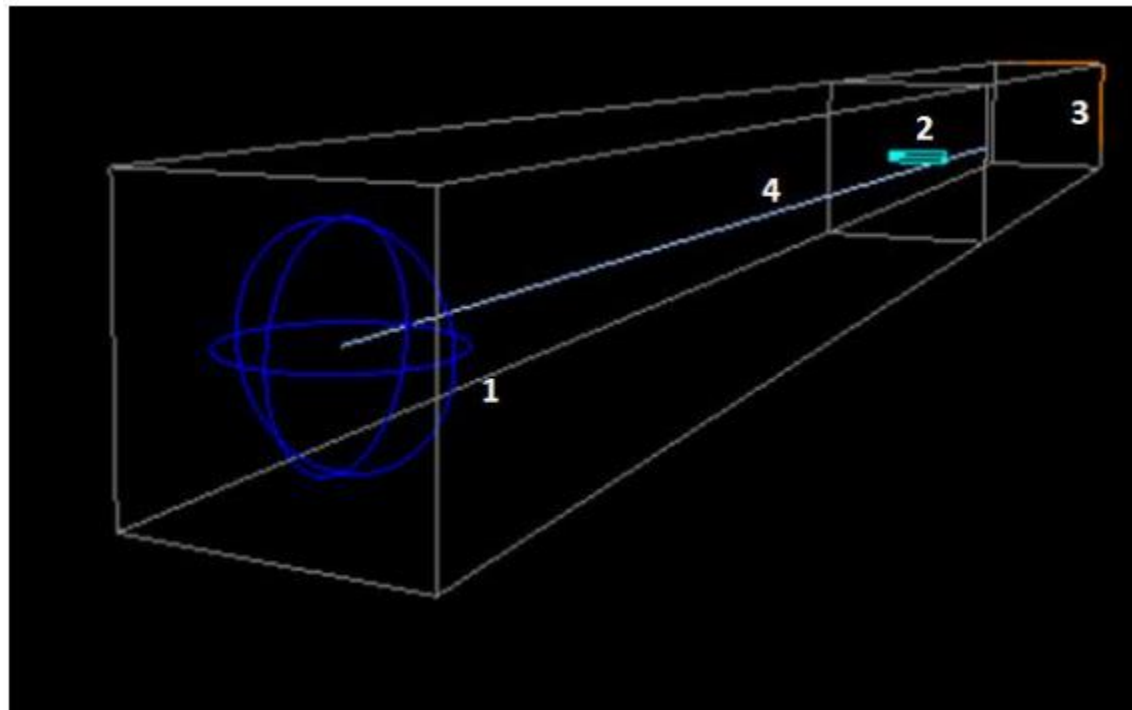
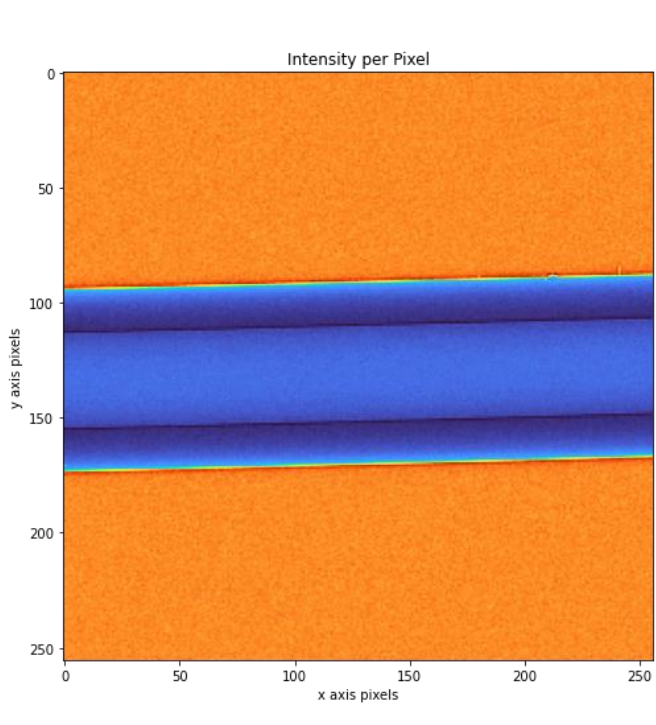


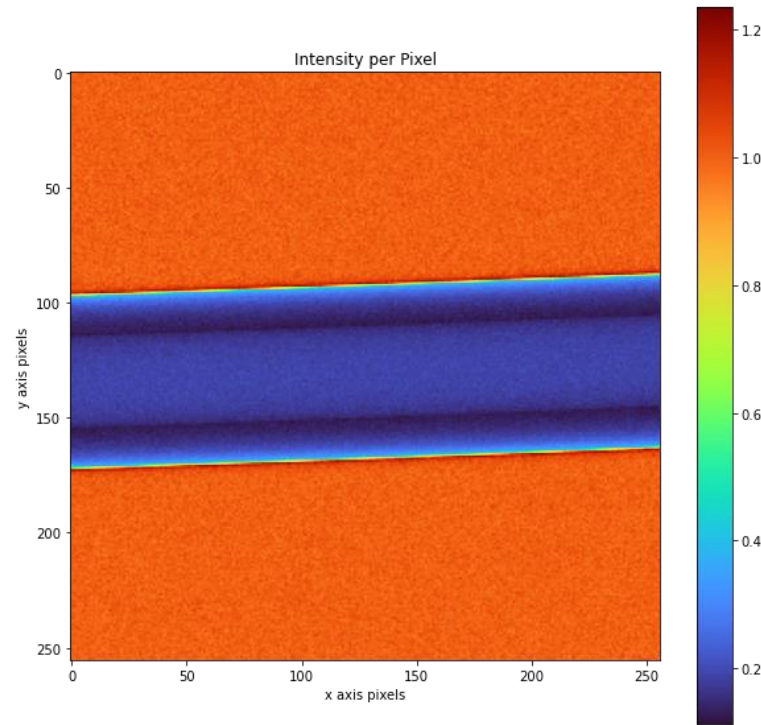
Figura 19. Simulated set-up

# Experimental Results

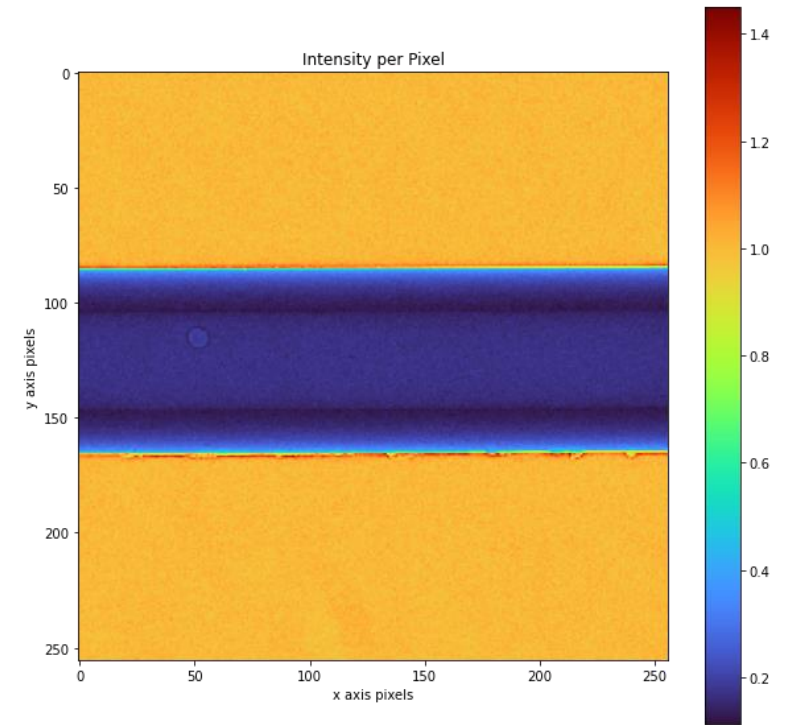
1.43 mm samples



**Air**



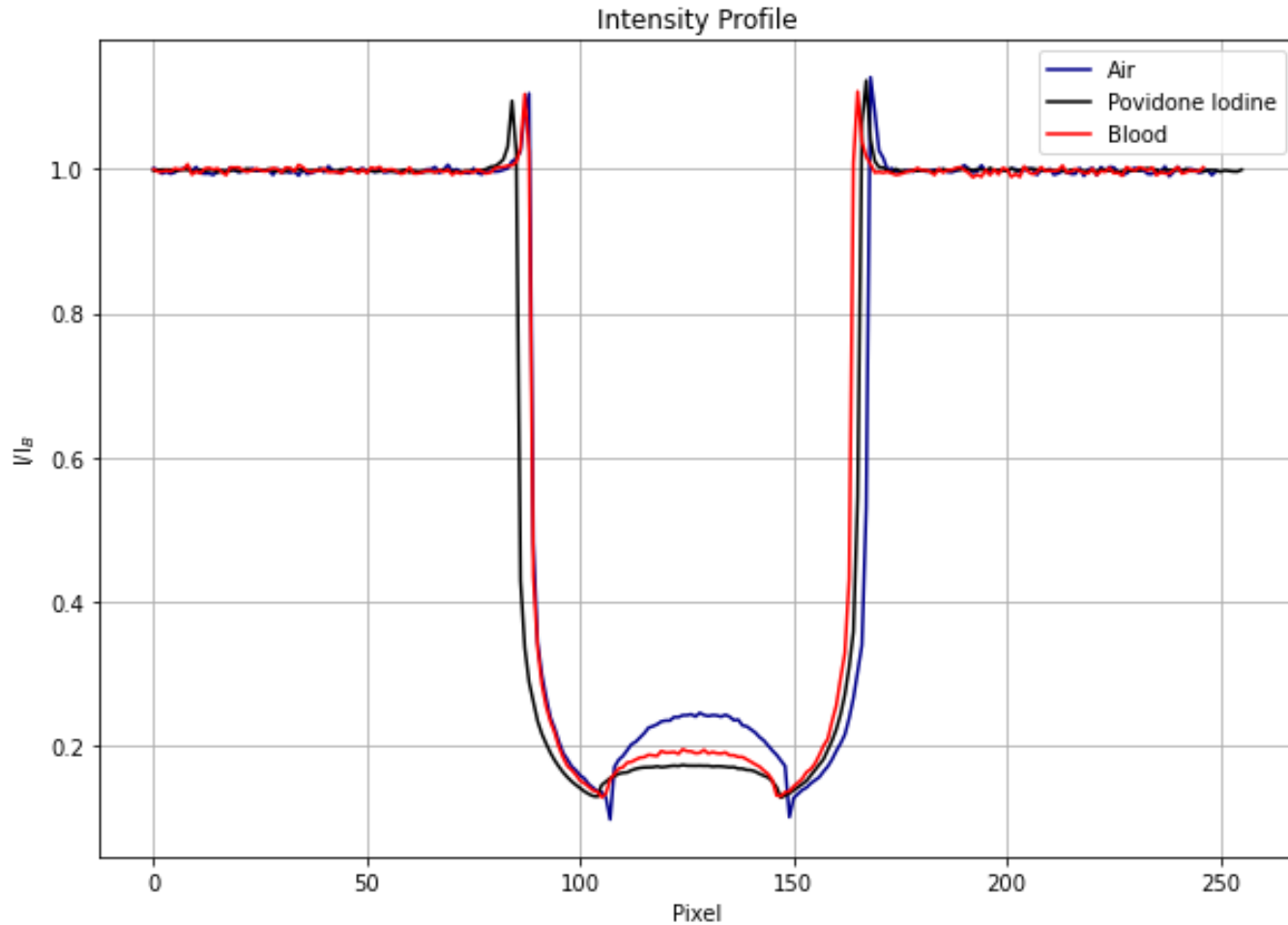
**Blood**



**Povidone iodine**

# Experimental Results

1.43 mm samples

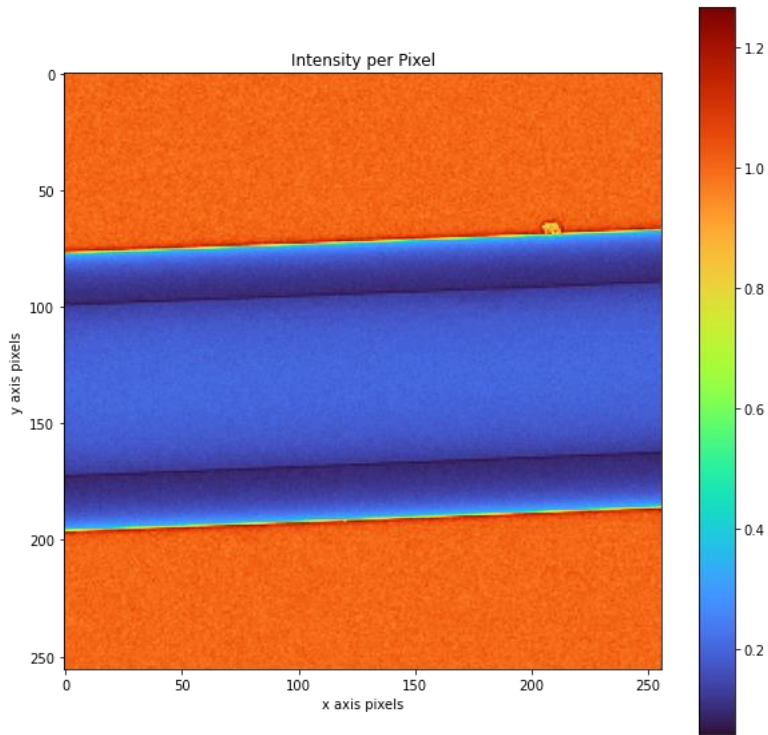


Filling Material	CNR
Air	$35.8 \pm 1.8$
Blood	$29.9 \pm 0.3$
Povidone Iodine	$87.6 \pm 5.4$

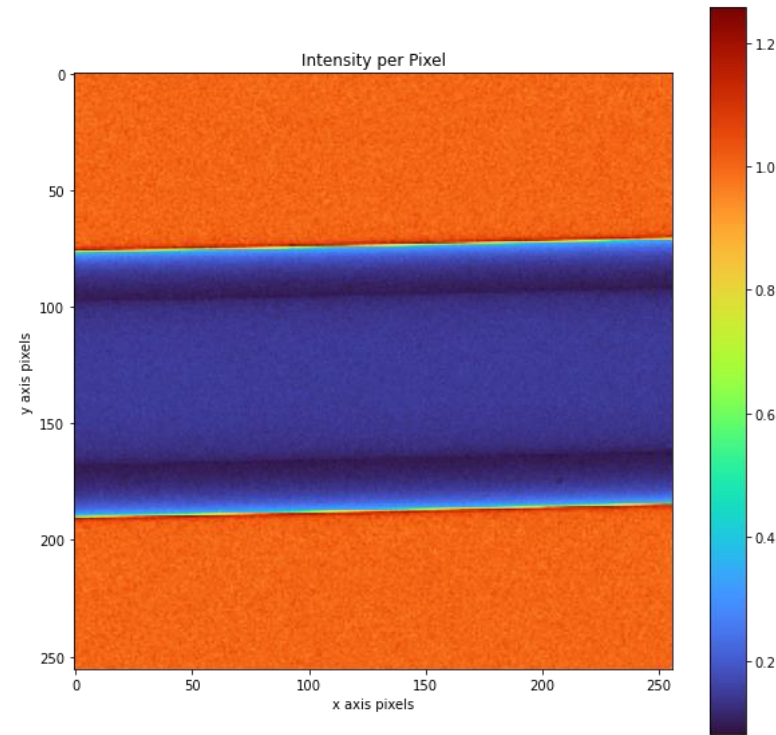


# Experimental Results

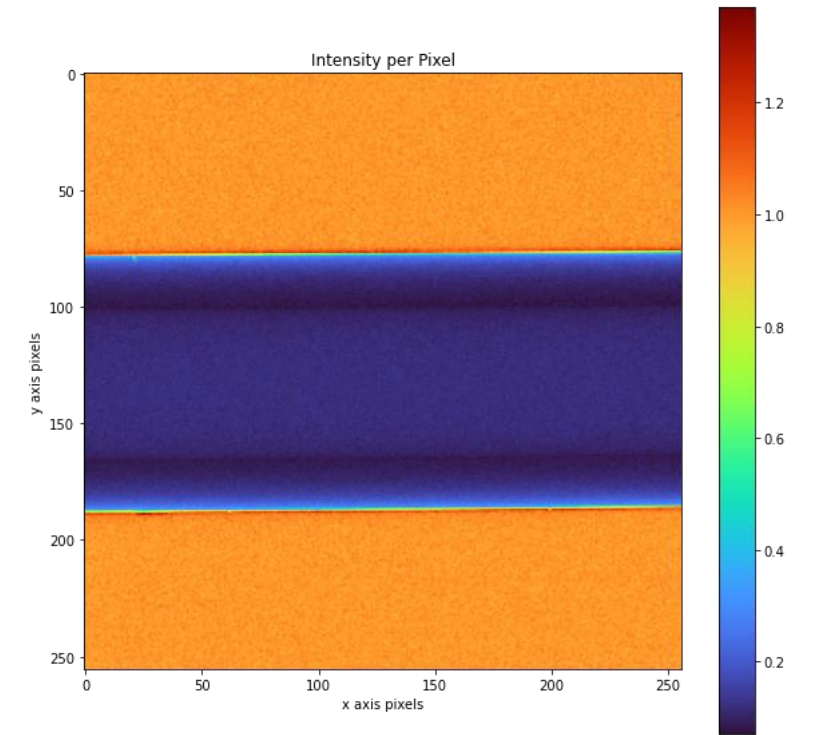
2.00 mm samples



Air



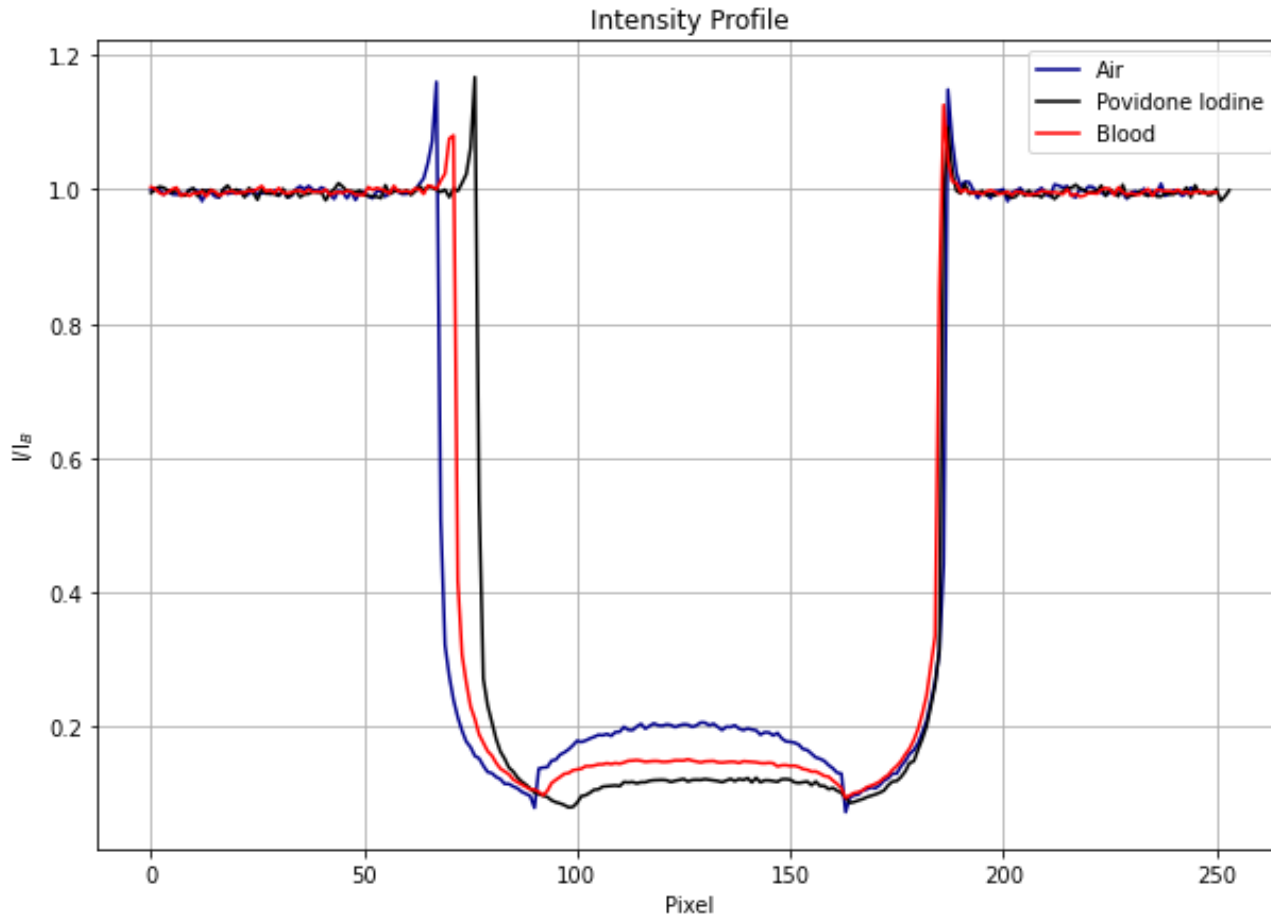
Blood



Povidone iodine

# Experimental Results

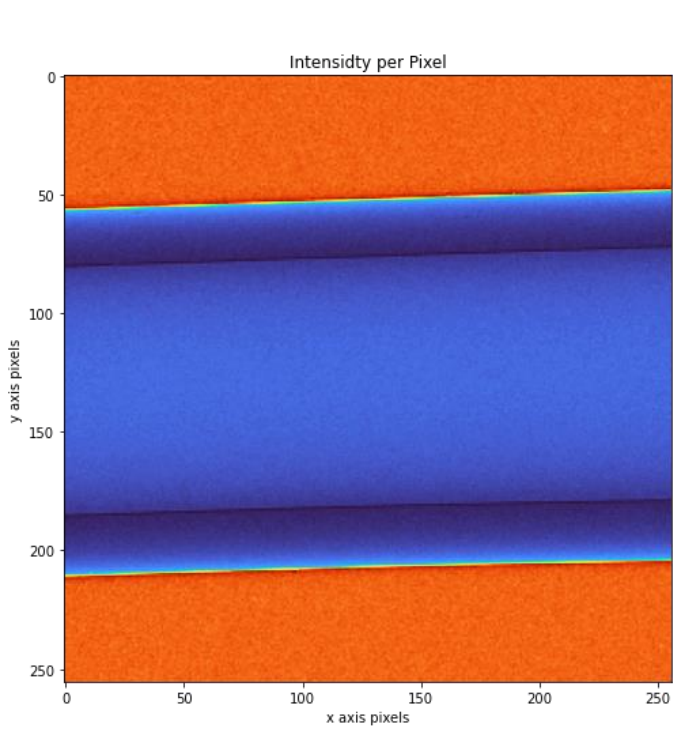
2.00 mm samples



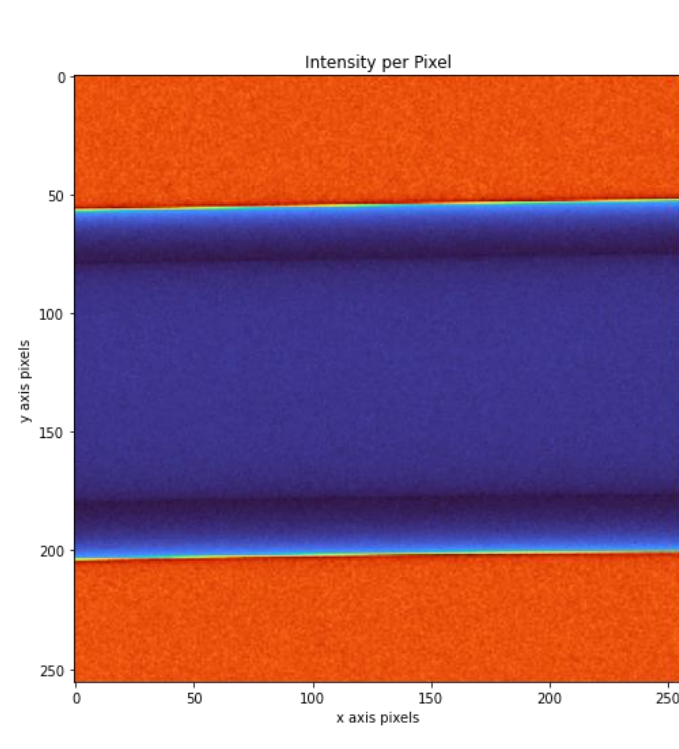
Filling Material	CNR
Air	$29.8 \pm 0.6$
Blood	$34.8 \pm 3.5$
Povidone Iodine	$27.4 \pm 3.4$

# Experimental Results

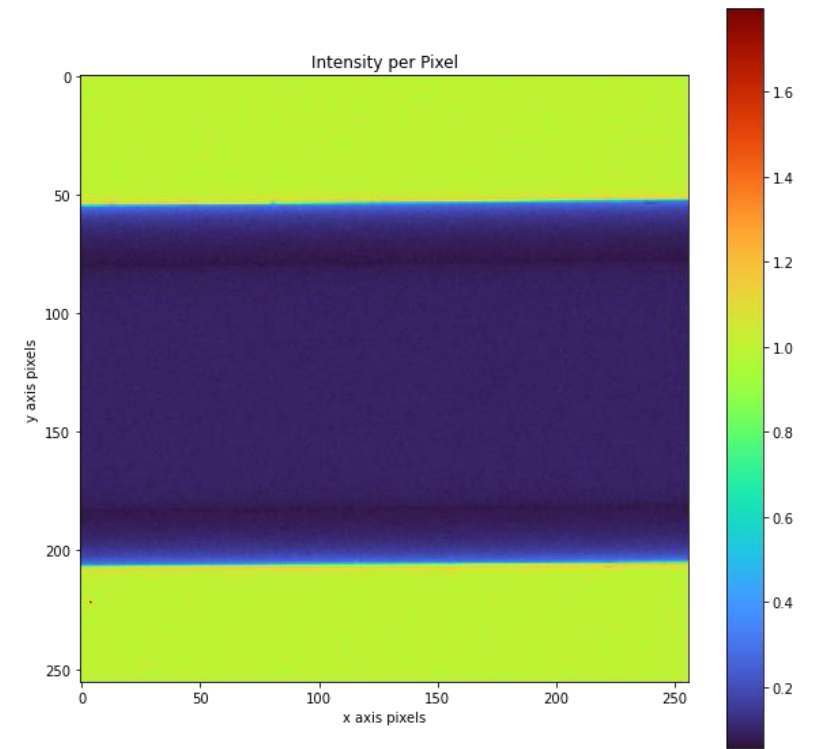
2.54 mm samples



Air



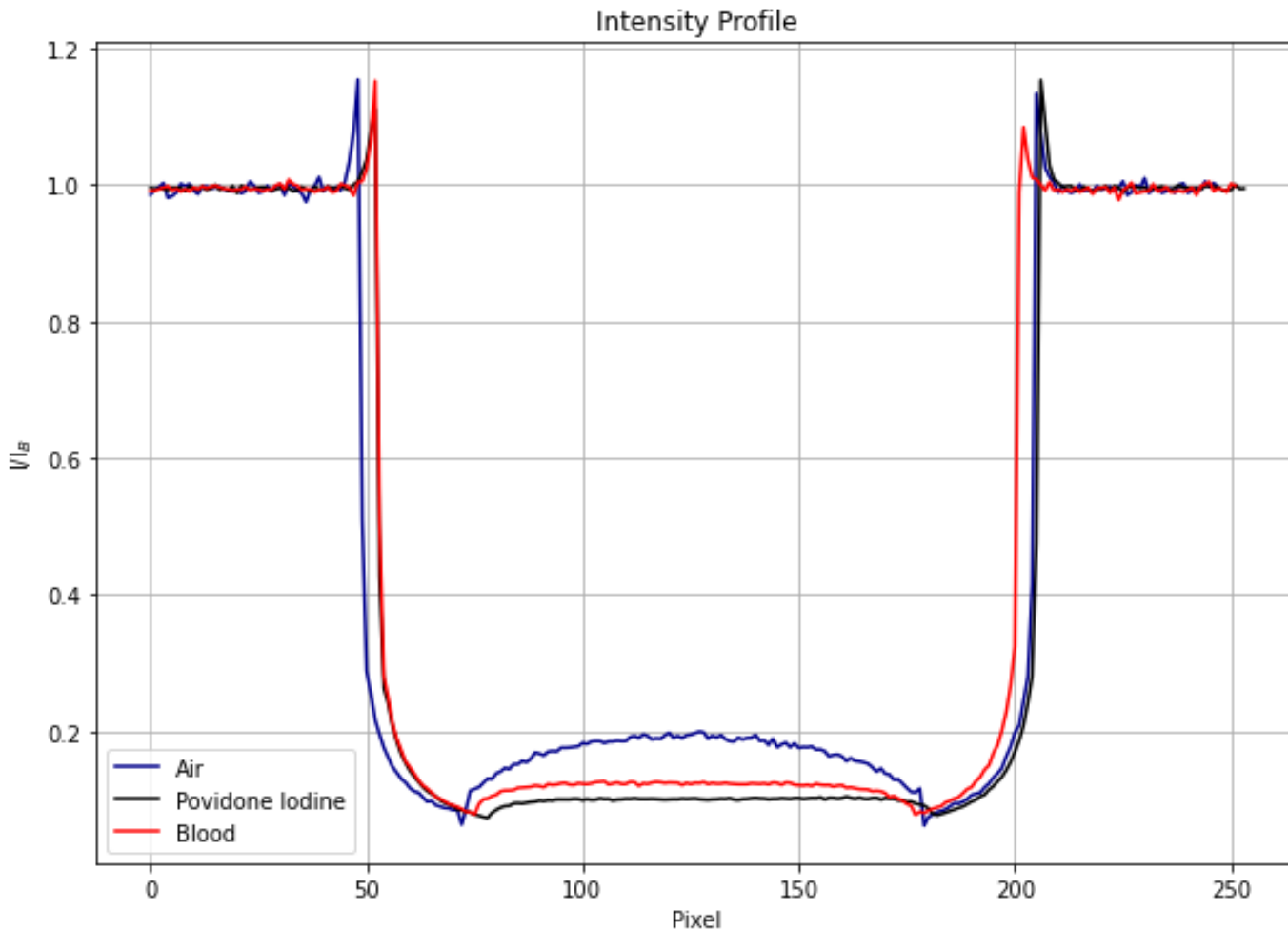
Blood



Povidone iodine

# Experimental Results

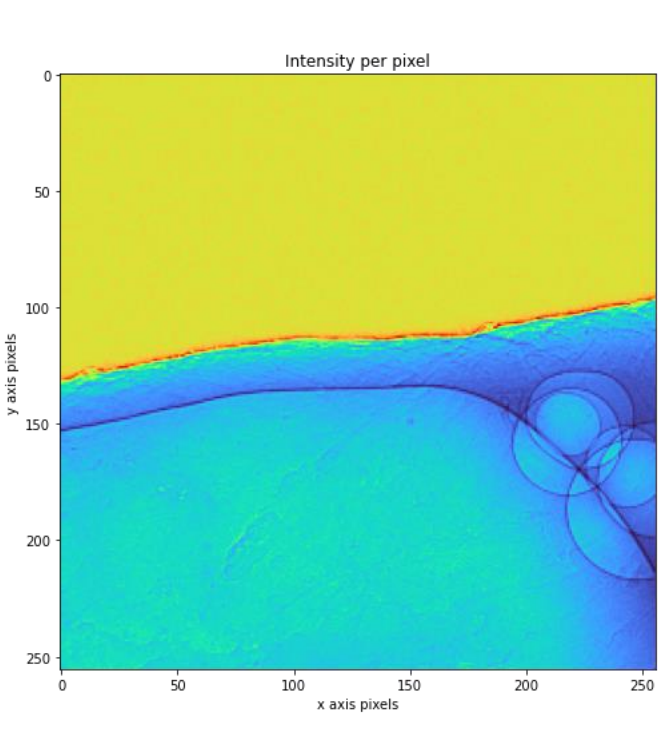
2.54 mm samples



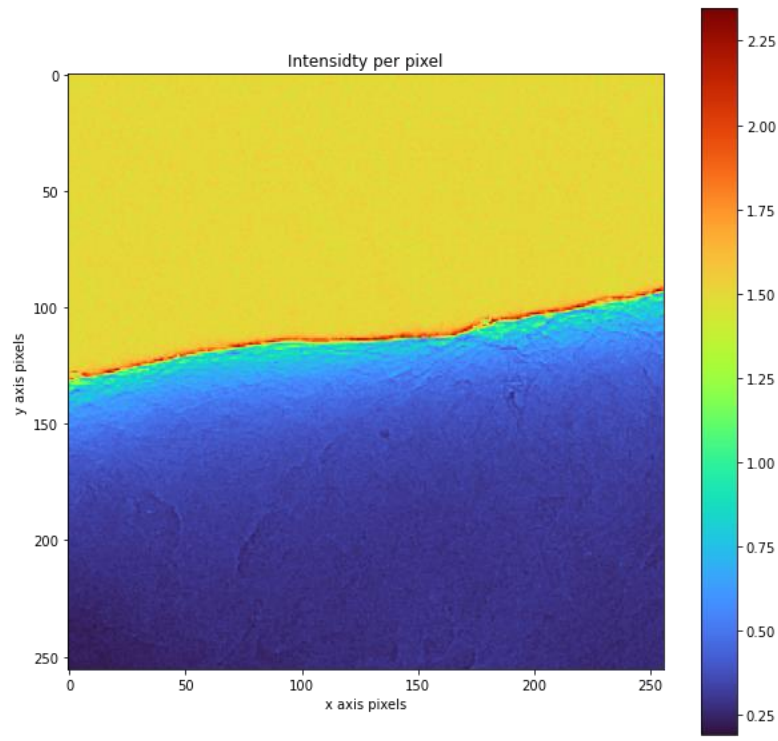
Filling Material	CNR
Air	$24.4 \pm 2.2$
Blood	$30.2 \pm 4.5$
Povidone Iodine	$56.2 \pm 4.0$

# Experimental Results

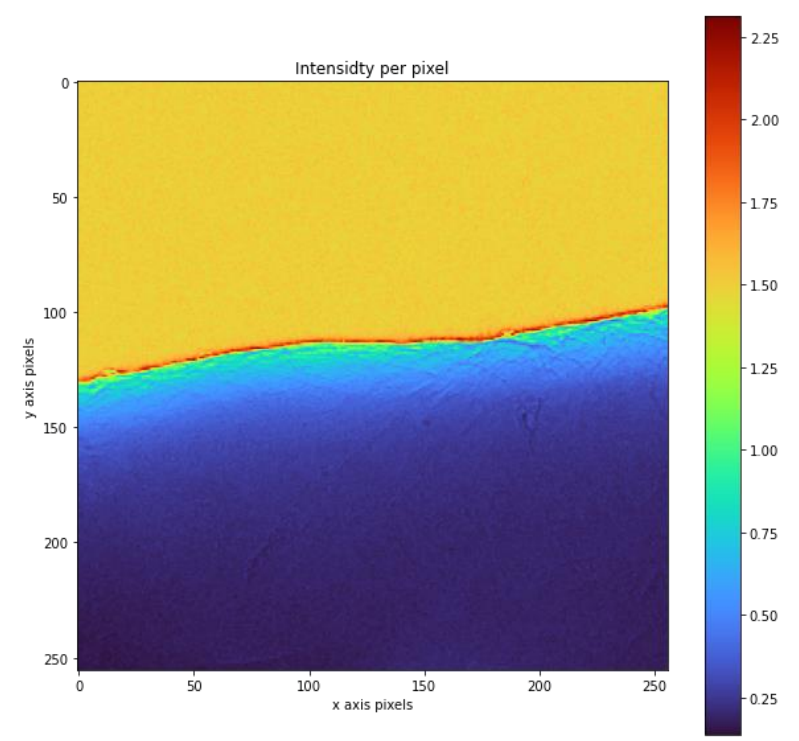
## Pig Aorta



Air



Blood



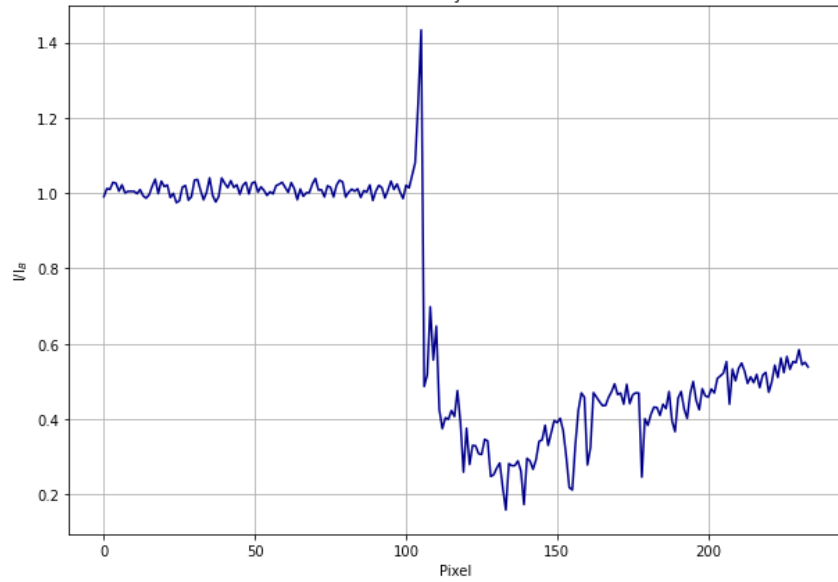
Povidone iodine

# Experimental Results

## Pig Aorta

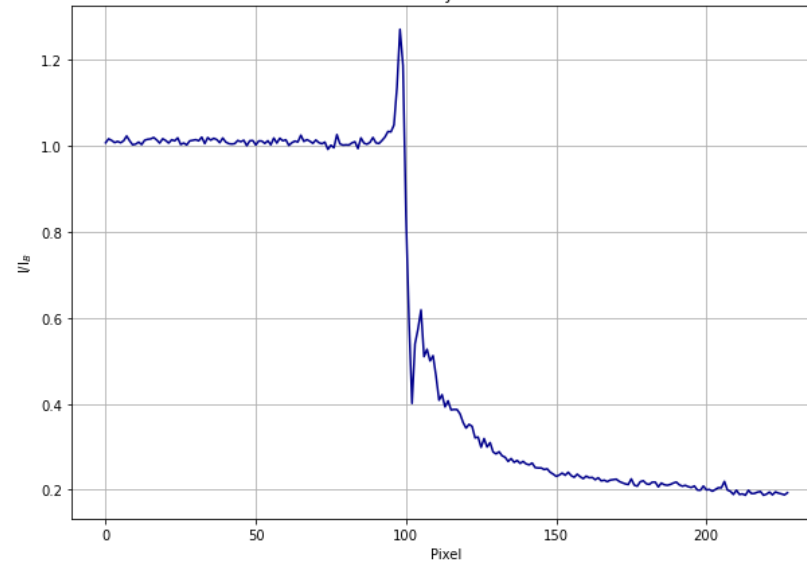
**Air**

Intensity Profile



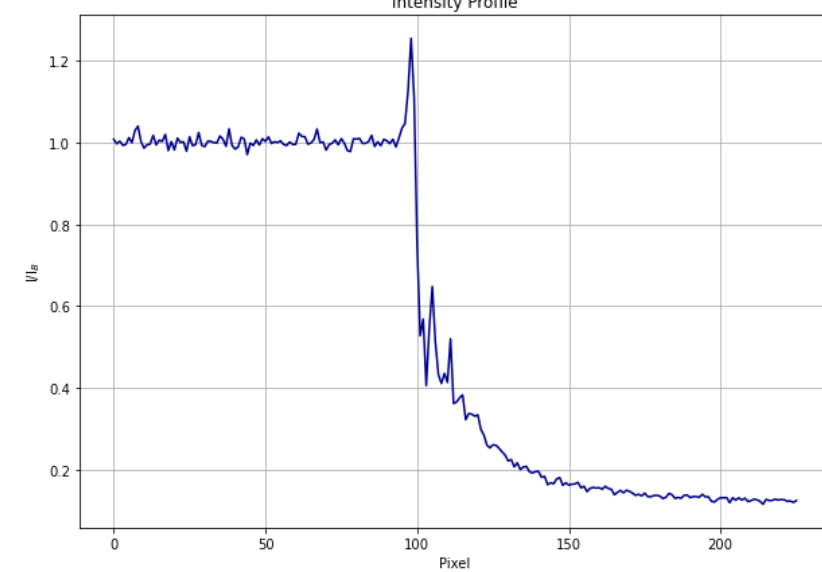
**Blood**

Intensity Profile



**Povidone iodine**

Intensity Profile



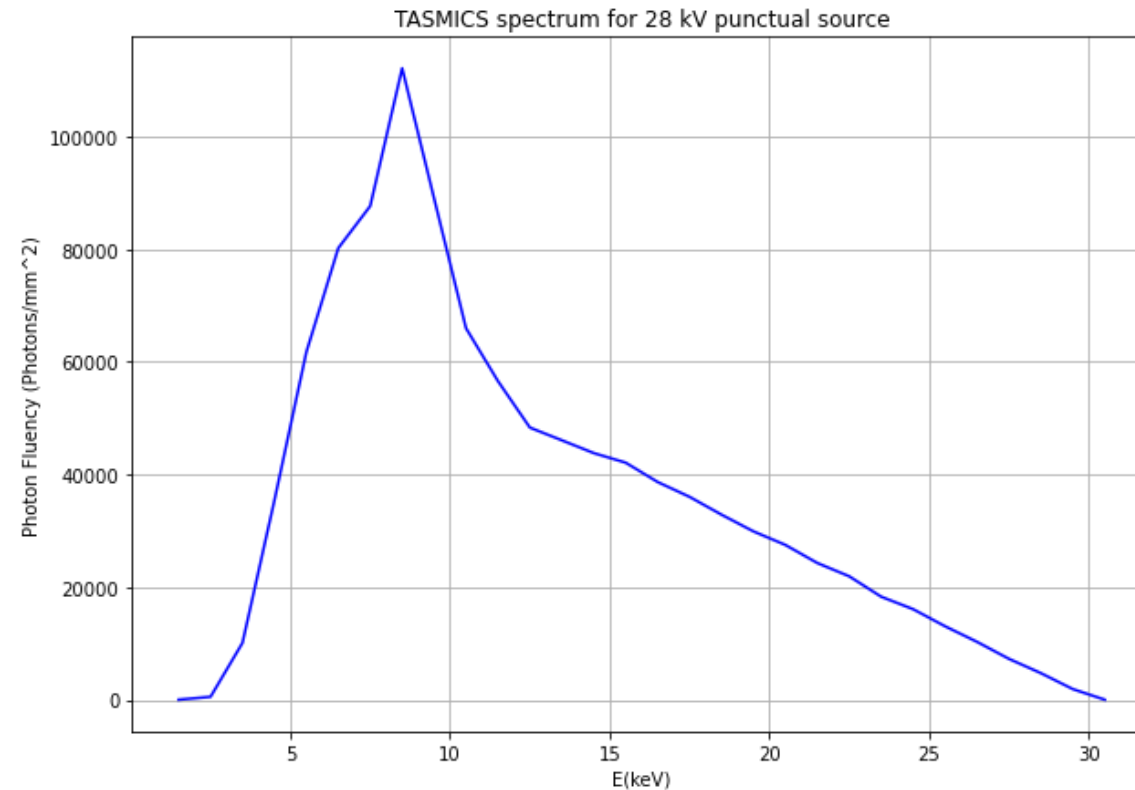
Filling Material	CNR
Air	26.8
Blood	43.3
Povidone Iodine	19.9

# Computational Results

**Sample:** PVC tube of various external diameters, filled with blood, 60 cm from the source

**Fuente:** Punctual, with energetic spectrum, covers detector width

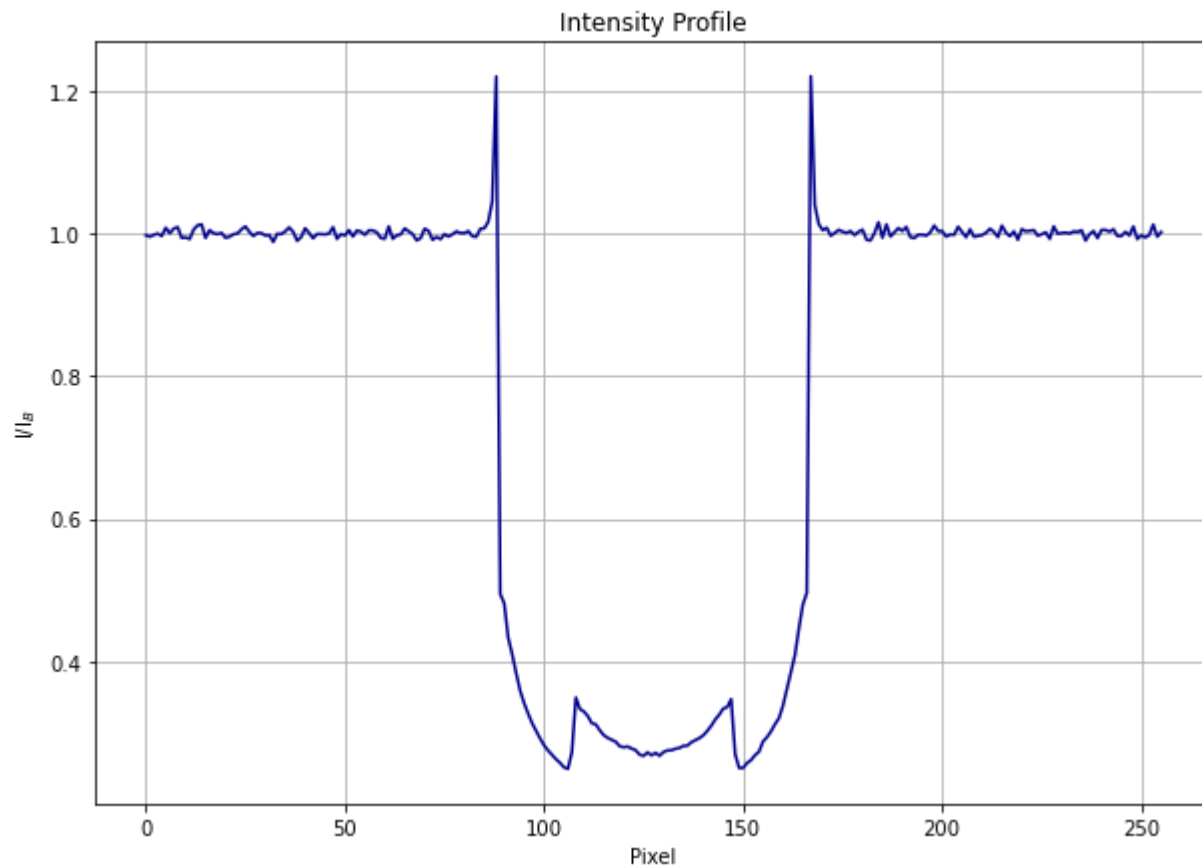
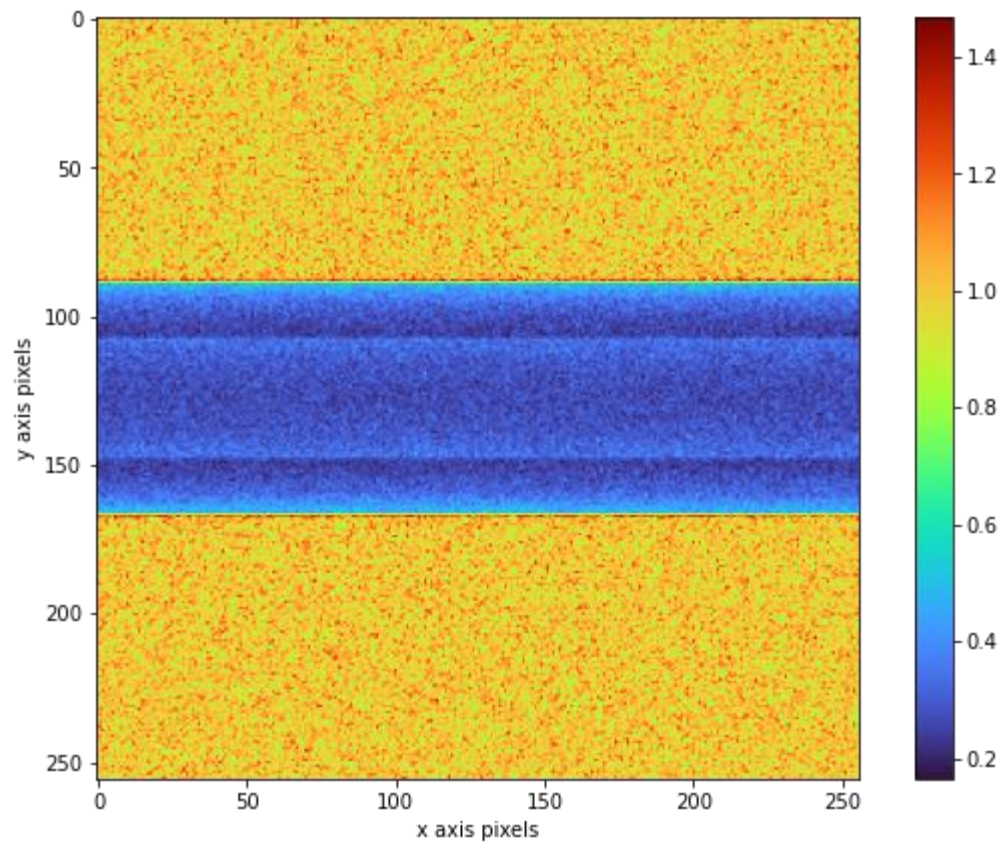
**Detector:** 256 x 256 pixel matrix, 55  $\mu\text{m}$  sideways, 1.80 m from the source



# Computational Results

1.43 mm sample

$10^7$  photons



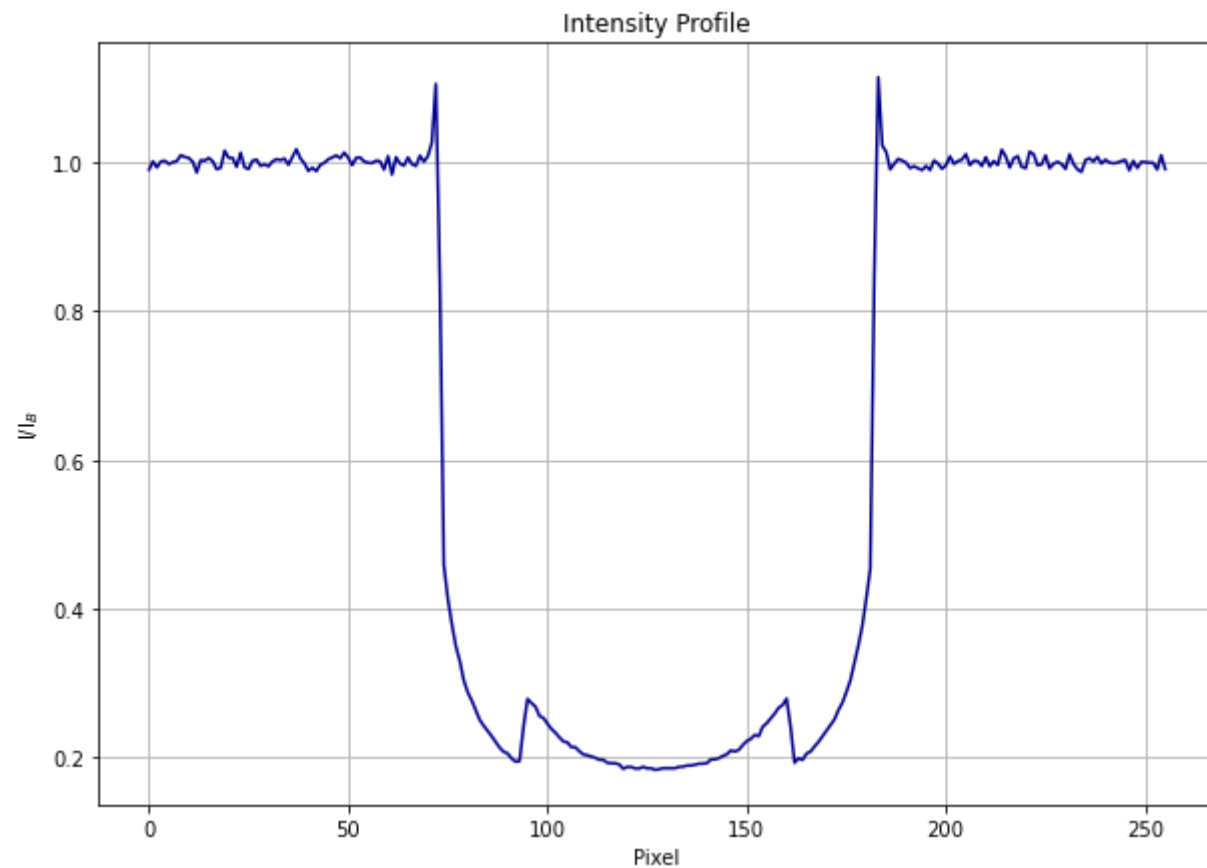
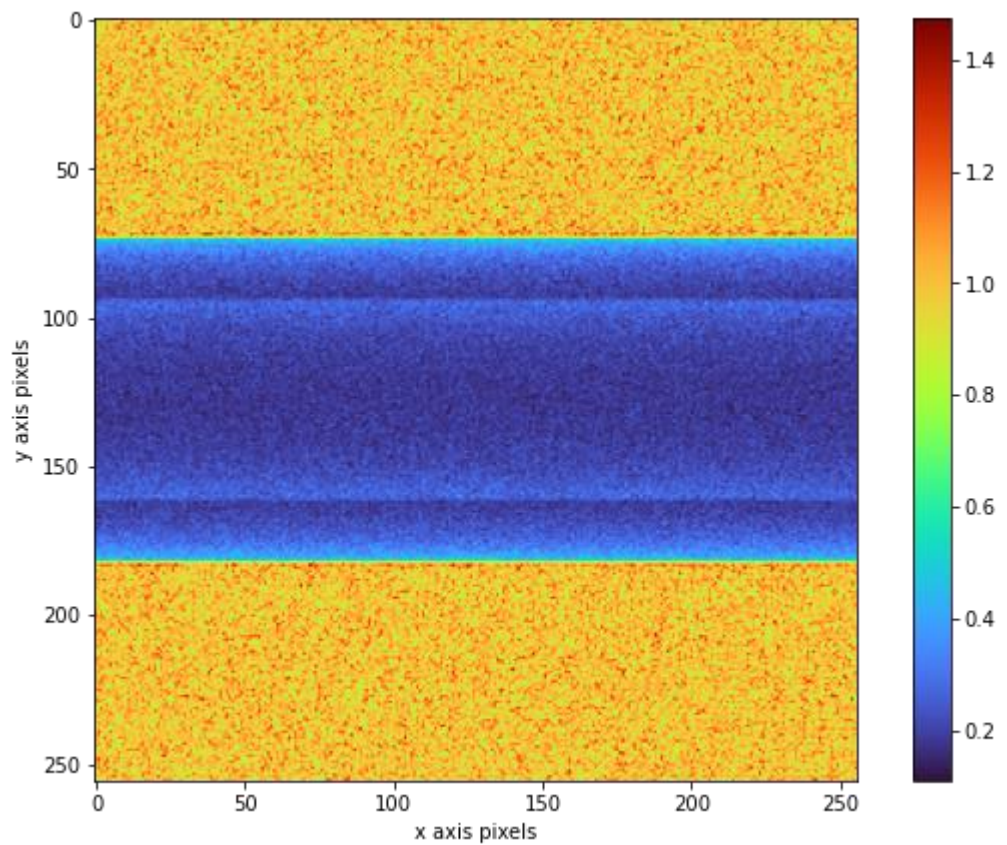
CNR = 41.1



# Computational Results

2.00 mm sample

$10^7$  photons

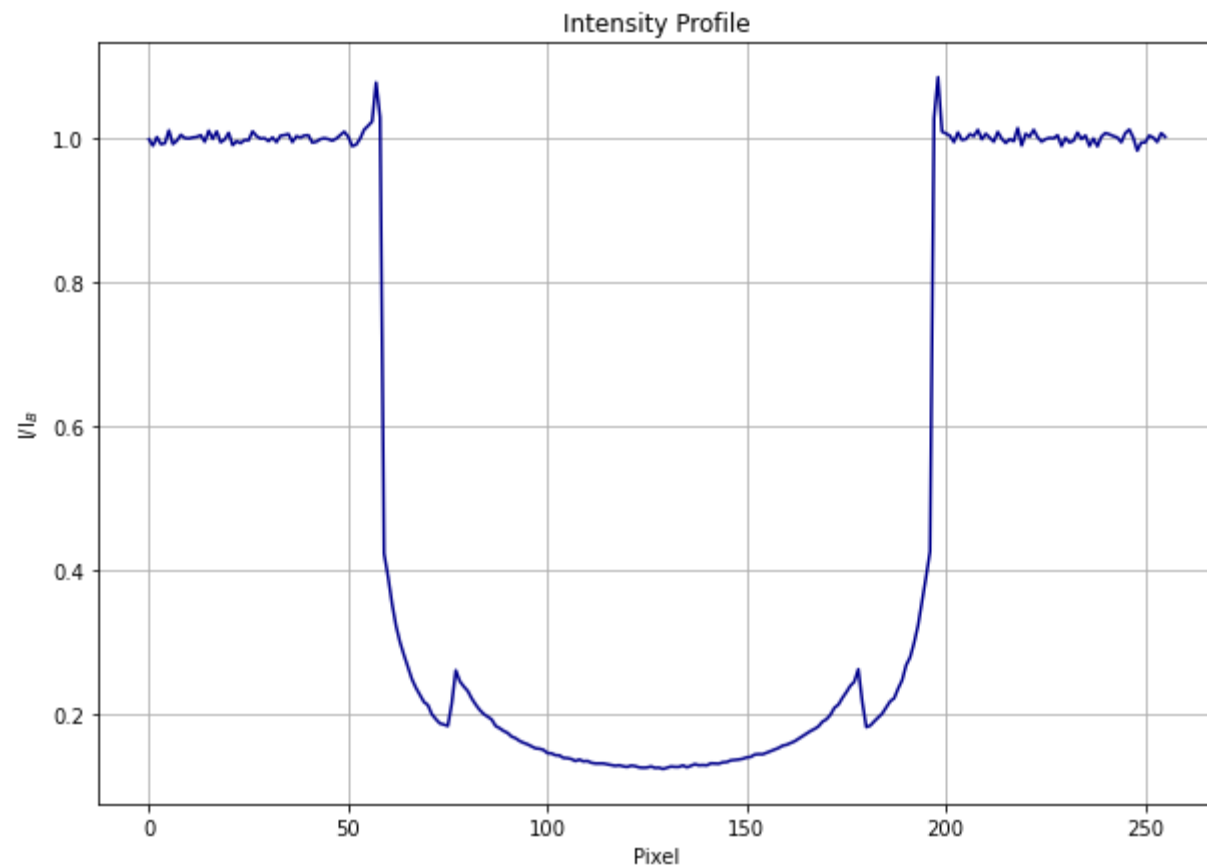
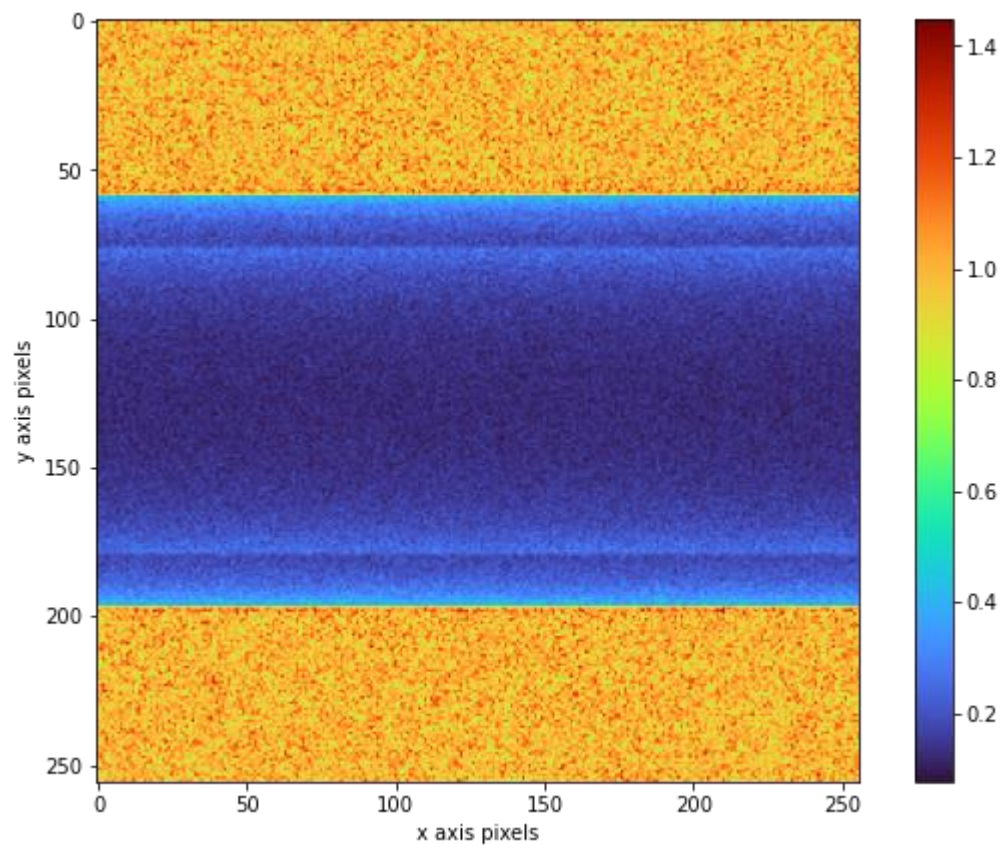


CNR = 15.9

# Computational Results

2.54 mm sample

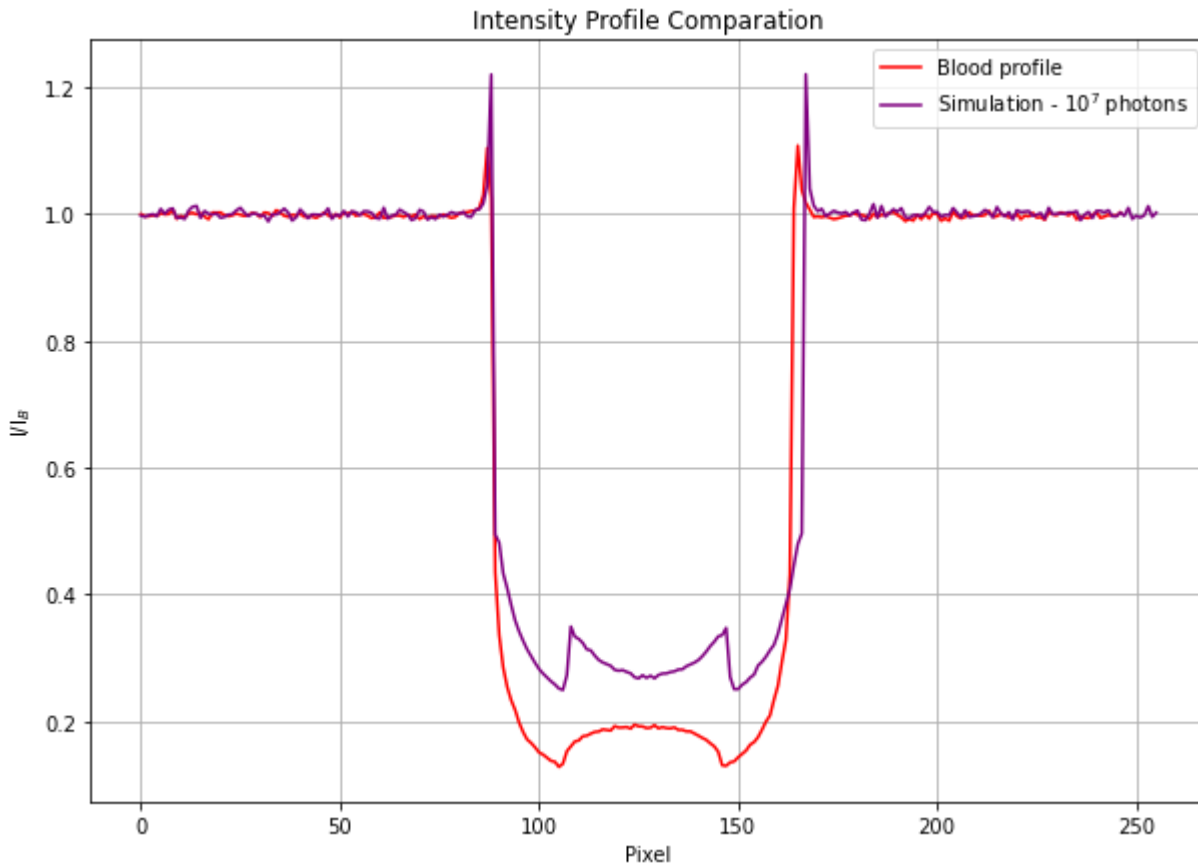
$10^7$  photons



CNR = 14.6

# Experimental and computational comparison

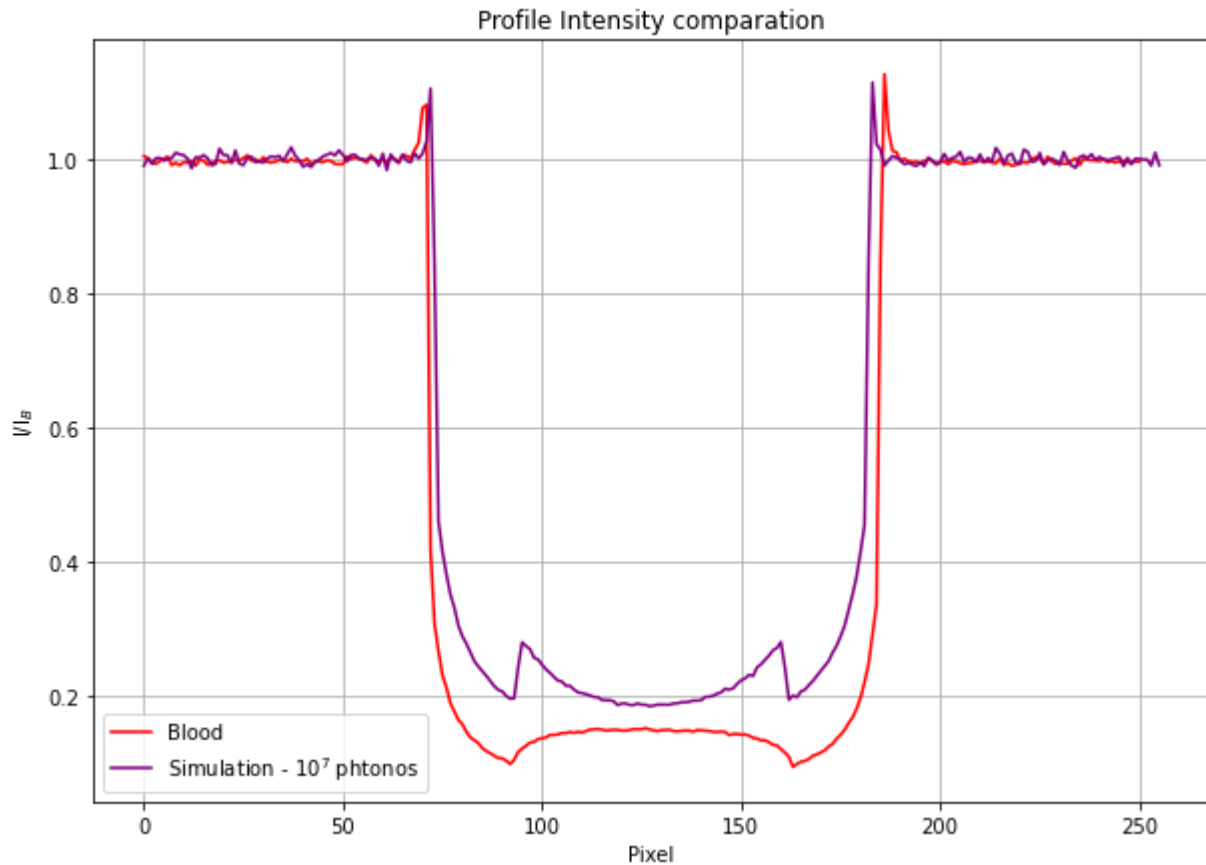
1.43 mm samples



Method	$\sigma_B$	$I_{max}$	CNR
Experimental	$3.56 \times 10^{-3}$	1.11	29.9
Simulation	$5.34 \times 10^{-3}$	1.22	41.1

# Experimental and computational comparison

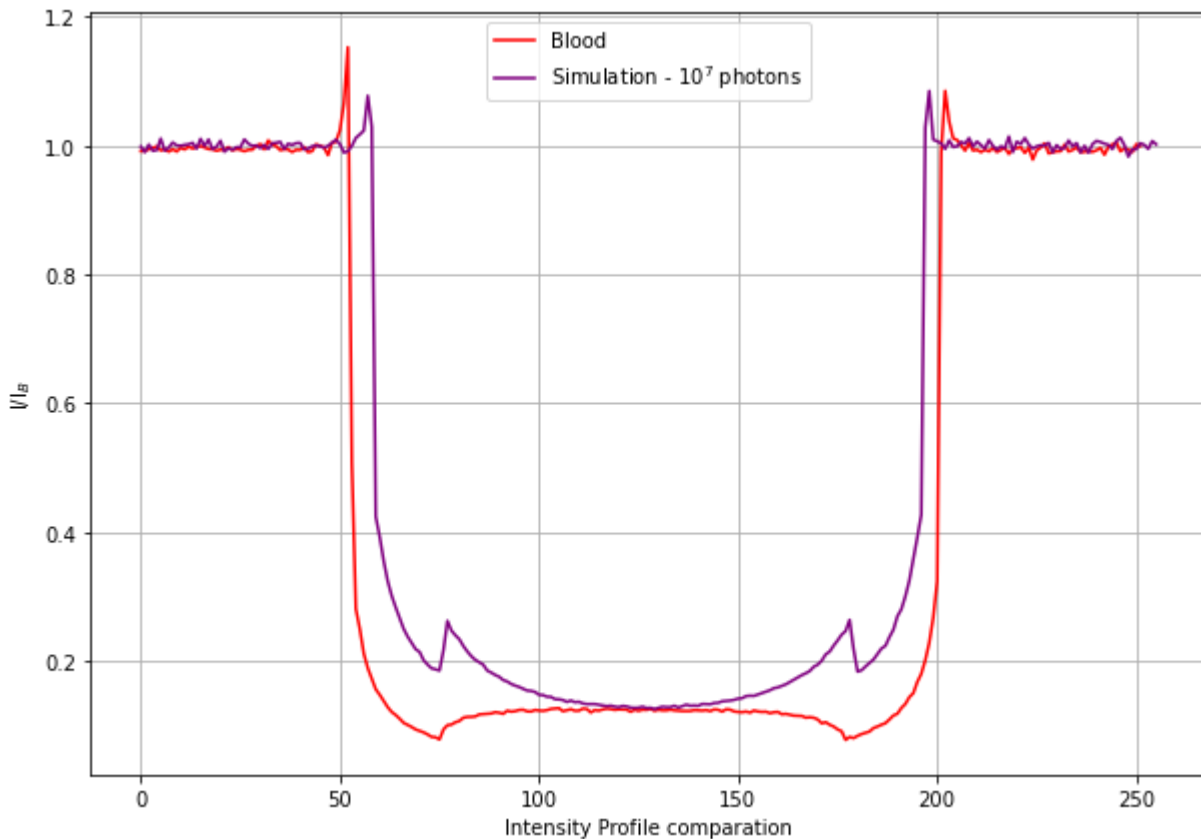
2.00 mm samples



Method	$\sigma_B$	$I_{max}$	CNR
Experimental	$3.38 \times 10^{-3}$	1.10	34.8
Simulation	$6.87 \times 10^{-3}$	1.11	15.9

# Experimental and computational comparison

2.54 mm samples



Method	$\sigma_B$	$I_{max}$	CNR
Experimental	$4.62 \times 10^{-3}$	1.12	30.2
Simulation	$5.91 \times 10^{-3}$	1.08	14.6

# Conclusions

- An exhaustive compilation of the literature related to XPCi methods applied to various areas, including the visualization of veins and arteries, was carried out.
- A computational and laboratory study of the X-ray phase contrast imaging method could be carried out, where in both cases CNRs of the same order of magnitude were obtained.
- The phase contrast effects were visualized in the organic (pig artery) and inorganic (PVC tubes) samples analyzed in the high energy laboratory of the Universidad de los Andes.
- Simulations were carried out that reproduce the setup carried out experimentally, obtaining highly similar results.
- A user guide was developed for the McXtrace software that enables X-ray phase contrast simulations to be performed.

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